# First Results from a Test Bench for Very High Resolution Small Animal PET Using Solid-State Detectors

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for

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# **Resolution Limitations for Conventional PET**

### **Inter-Crystal Scattering**

### **Scintillator**



- Multiple Interactions
- Energy deposited over a volume
- ~ 1 cm mean path

### Depth of Interaction Uncertainty



- Penetration into crystals widens LOR
  - Best Resolution ~ 1-2 mm

# **Compton PET Concept**



**Si-Si** Uses tw**Sesteisivity**dettectors: ow reso**FUNDM**and3AigM

Low respinction detectors can be conventionality EP-01% small animal PEWEMan-7290 µm

**BGO-BGO** High resolutionvideteetors stack of **FWHHMD=-\$645**sitime solid-state detectors

\* Not including effects of annihilation photon acolinearity and positron range Resolution to challenge positron range

# **Compton Pet Test Bench**

### Silicon detector



### **BGO** detector



4.5 cm  $\times$  2.2 cm and 1 mm thick 32×16 (512) pads, 1.4 mm  $\times$  1.4 mm pixel size Energy Resolution 1.39 keV FWHM for Tc 99m

5.3 cm × 5 cm and 3 cm thick 8×4 array, 12.5 mm × 5.25 mm crystal size Energy Resolution 22% FWHM for Na-22

### Setup and Alignment



BGO detectors, electronics not shown

# **Images of Two Point Sources**

**Compton PET** 

### **MicroPET R4**



### **ML-EM** Image reconstruction with **Si-Si** coincidence events only

## **Compton PET: Intrinsic Resolution**





Needle 25G (ID = 0.254 mm, OD = 0.5mm, SS\_steel wall = 0.127 mm)





Image Resolution = 700 μm FWHM

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### **Compton PET: Resolution Uniformity**



## Summary of Current Situation

- Both simulation as well as experimental results confirm Compton (or Silicon) PET concept.
- Testbench resolution 700 µm FWHM better than the resolution we were able to achieve with a commercial mircoPET R4 system using the same test object and even better reconstruction software.
- Uniform resolution over the entire Field of View.

Next Steps: Use the test setup to study some of the limitations of this concept.

### Limitation 1: Silicon Detector Time Resolution



FWHM = 78.7 ns (due to Time Walk) Timing window = 200 ns

[see Poster J03-24 for more details]

### Measurement of Silicon Detector Time Resolution



## Time Walk: LE versus CFD



## Limitation 2: Positron Range Distribution

#### **Positron Annihilation Point Distribution**

# Distribution of Positron Range



#### [by Levin and Hoffman]

	<b>F-18</b>	<b>C-11</b>	N-13	O-15	
Max energy (MeV)	0.64	0.97	1.19	1.72	
Mean energy (MeV)	0.25	0.39	0.49	0.74	
FWHM (mm)	0.10	0.19	0.28	0.50	
FWTM (mm)	1.03	1.86	2.53	4.14	

#### Spatial resolution (FWHM [mm])

Event	Geometric		Overall					
	+ Acolinearity	<b>F-18</b>	C-11	<b>N-13</b>	O-15			
Si-Si	0.241	0.393	0.443	0.492	0.553			
Si-BGO	0.816	1.062	1.261	1.419	1.742			
BGO-BG	O 1.458	1.977	2.270	2.490	3.069			

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## Revisiting an Old Idea

- Embed PET FOV in strong magnetic field (Raylman, Hammer, etc.)
- Positrons spiral and range is reduced transverse to B-field vector
- Not very effective for F-18 positrons
- Potentially useful for emitters with higher endpoint energies (I-124, Tc-94m, etc.) Increasingly being used in small animal imaging



### Simulated Range Reduction for I-124

# Effect on Image Quality



Axially constant object transverse to B-field

## **Experimental Verification**



### Combine Compton PET with 8 T MRI system at OSU Medical School



# **Compton PET Summary**

- In order to achieve sub-millimeter spatial, a small animal PET based the Compton PET concept was developed.
- Simulation results demonstrated sub-millimeter spatial resolution of the Compton PET (0.4 mm FWHM from Si-Si and 1.0 mm FWHM from Si-BGO).
- Experimental results with a prototype setup using 1.4 mm x 1.4 mm x 1 mm silicon pads verified very high resolution (700 μm FWHM).
- Experimental results demonstrate the Si pad detector time resolution can be better than 10 ns.

# and Outlook

- Test setup to operate Compton PET prototype in an 8 T MRI system in preparation.
- Development of a new ASIC with significantly reduced time walk jitter underway.

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# **Additional Transparencies**

### Scatters and DOI Uncertainty Problem in a BGO PET

- EGS4 Monte Carlo simulations
- BGO PET (17.6 cm I.D. 16 cm length segmented with 3 mm x 3mm x 20 mm crystals)
- Point sources at 0, 3, 6, 9, 12, 15, and 18 mm from center of FOV
- Filtered back projection reconstruction

**True first interaction position** 



#### Centroid of scattered E distribution



DOI uncertainty included in *both* images

### **Energy Resolution of Si Pad Detector**



### Am-241 (59.5 keV)



FWHM = 1.49 keV (2.5 %)

#### Si(OH1) + Source(Tc-99m) 2000 1800 1600 1400 1200 FWHM = 1.3864 keV 1000 Counts 800 600 400 200 20 40 60 120 160 180 80 100 140 Energy (keV)

Tc-99m (140.5 keV)

FWHM = 1.39 keV (0.99%) Pb Kα1 = 74.969 keV, Kα2 = 72.804 keV, Kβ1 = 84.936 keV, and Compton edge = 49.8 keV

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## Simulated ComptonPet Image

- Combined with Maximum likelihood Expectation Maximization (ML-EM)
- Iteration number = 200



Si-Si (160k) + Si-BGO (1.4M) + BGO-BGO (3.1M)

### **Coincidence Events**



Noise Equivalent Count Rate (NECR)



### **Compton Kinematics**



### **Improvement of NECR using Compton Kinematics**

Si-Si

Si-BGO

**BGO-BGO** 



A = 0.1 mCi, Si = 5 ns FWHM, BGO = 1 e/ns,

E\_W = ±50 %, T\_W = 7 ns, A\_W (Si-Si) = ±5 degree, A\_W (Si-BGO) = ±7.5 degree

Improvement: Maximum 86 % for Si-Si and 36 % for Si-BGO at 5 mCi